

1 **TITLE:** Sperm selection by rheotaxis improves sperm quality and early embryo  
2 development.

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26

27 **ABSTRACT**

28 The objective of this work was to elucidate whether a sperm selection method that  
29 combines rheotaxis and microfluidics can improve the selection of spermatozoa over  
30 density gradient and swim-up. For this purpose human sperm selected by rheotaxis were  
31 compared against density gradient, swim-up and a control group of non-selected  
32 spermatozoa in split frozen-thawed (FT) and fresh (F) semen samples. Sperm quality  
33 was assessed in terms of motility, morphology, DNA fragmentation index (DFI),  
34 viability, acrosome integrity and membrane fluidity. Using a mouse model, we  
35 compared fertilization and embryo development rates after performing ICSI with  
36 spermatozoa sorted using rheotaxis or swim-up. Selection by rheotaxis yielded a sperm  
37 population with reduced DFI than the control ( $P<0.05$ ), improved normal morphology  
38 ( $P<0.001$ ) and higher total motility (TM;  $P<0.001$ ) than the other techniques studied in  
39 F and FT samples. Swim-up increased TM compared to density gradient and control in  
40 FT or F samples ( $P<0.001$ ), and yielded lower DFI than the control with F samples  
41 ( $P<0.05$ ). In FT samples, selection by rheotaxis yielded sperm with higher viability than  
42 control, density gradient and swim-up ( $P<0.01$ ) while acrosomal integrity and  
43 membrane fluidity were maintained. When mouse spermatozoa were selected for ICSI  
44 using rheotaxis compared to swim-up, there was an increase in fertilization ( $P<0.01$ ),  
45 implantation ( $P<0.001$ ) and foetal development rates ( $P<0.05$ ). These results suggest  
46 that, in the absence of non-destructive DNA testing, positive rheotaxis can be used to  
47 select a population of low DNA fragmentation spermatozoa, with high motility,  
48 morphology and viability, leading to improved embryo developmental rates.

## 49 INTRODUCTION

50 Intracytoplasmic sperm injection (ICSI) was initially developed for patients with severe  
51 male factor infertility, but its application has widened for cases with low oocyte yields,  
52 cryopreserved oocytes, insemination for patients at risk for HIV or even to comply with  
53 laws that limit the number of eggs to be inseminated (Palermo *et al.*, 2017). Recent  
54 reports on the use of assisted reproductive technology (ART) show a dominance of ICSI  
55 over conventional *in vitro* fertilization (IVF) and now makes up approximately 70% of  
56 all fertilizations *in vitro* (Adamson *et al.*, 2018; De Geyter *et al.*, 2020) despite major  
57 country to country variations.

58

59 The existing technologies used to select better quality spermatozoa for use in both IVF  
60 and ICSI involve sperm cells either being forced to swim through a density gradient  
61 using centrifugation or swim upwards in a tube of sperm preparation medium. These  
62 techniques have been used for decades in the preparation of spermatozoa for traditional  
63 IVF and by default are being used for sperm selection for ICSI as well, but seem to be  
64 suboptimal for this purpose (Oseguera-López *et al.*, 2019). Embryologists must then  
65 select through visual observation the best spermatozoon based on their morphology, a  
66 step that can be extremely time-consuming (Auger *et al.*, 2016; Sikka and Hellstrom,  
67 2016). In addition, they have no information on the DNA integrity of the selected sperm  
68 as there is no non-destructive test for DNA fragmentation.

69

70 The capacity of human spermatozoa to produce a good-quality embryo with a high  
71 implantation and development potential depends on many factors, including its DNA  
72 integrity (Miller *et al.*, 2010). High levels of DNA fragmentation in spermatozoa can  
73 slow down embryo morphokinetic parameters after ICSI (Wdowiak *et al.*, 2015) and

74 there is a positive relationship between levels of DNA damage in spermatozoa and  
75 spontaneous pregnancy loss (Robinson *et al.*, 2012). Up to 30% of patients seeking  
76 ART had high rates of sperm DNA breaks (Bungum *et al.*, 2004), and ICSI is the  
77 preferred method when DNA fragmentation index (DFI) exceeds 30% (Bungum *et al.*,  
78 2007; Chi *et al.*, 2017).

79

80 The need for a better sperm selection method has led to the development of new  
81 technologies to increase the quality of sperm selection for ICSI. Among others, sodium  
82 hyaluronate has been used to select spermatozoa based upon their maturity state in the  
83 form of droplets (Parmegiani *et al.*, 2010) or coating culture dishes (Worrilow *et al.*,  
84 2013); Magnetic activated cell sorting (MACS) combined Annexin V with magnetic  
85 beads to remove apoptotic sperm cells (Ziarati *et al.*, 2019), and a new group of devices  
86 have emerged to select spermatozoa based on microfluidics (Kishi *et al.*, 2015; Shirota  
87 *et al.*, 2016; Chinnasamy *et al.*, 2018; Nakao *et al.*, 2020).

88

89 Enroute to the site of fertilization in the ampulla, mammalian spermatozoa have the  
90 ability to be actively guided towards the oocyte by different mechanisms (Pérez-  
91 Cerezales *et al.*, 2015). Among them, rheotaxis - or swimming against a flow - has been  
92 revealed to be a long-distance biophysical guiding mechanism for human spermatozoa  
93 (Kantsler *et al.*, 2014). In a recent preliminary study by De Martin *et al.*, (2017), the use  
94 of a rheotaxis related sperm selection method resulted in an improvement in sperm  
95 morphology and chromatin maturity. However the study did not assess the impact of the  
96 selection method on DNA fragmentation or fertility potential of the selected sperm.

97

98 Here we report a new sperm selection method which combines, in a single-use  
99 microfluidic device, the ability of spermatozoa to orientate and swim against a flow of  
100 media using microfluidic technology. We compared sperm selection by rheotaxis using  
101 a proprietary designed microfluidic system with the current standard procedures for  
102 sperm selection, namely density gradient and swim-up. Sperm quality was assessed in  
103 terms of motility, morphology, viability, acrosome integrity, membrane fluidity and  
104 DNA fragmentation using frozen-thawed and fresh spermatozoa. Using a mouse model,  
105 we compared fertilization and embryo development rates after performing ICSI with  
106 spermatozoa sorted using rheotaxis or swim-up.

107

## 108 **MATERIALS AND METHODS**

109 Unless otherwise indicated, all chemicals were of analytical grade and obtained from  
110 Sigma Aldrich Ireland Ltd (Arklow, Ireland).

111

### 112 **Ethical approval**

113 All donors gave written informed consent and the use of human sperm samples for  
114 research was approved by Faculty of Science and Engineering Research Ethics  
115 Committee at the University of Limerick.

116

117 Experiments in mice were carried out in strict accordance with recommendations of the  
118 guidelines of European Community Council Directive 86/609/EEC. Every effort was  
119 made to minimize suffering. The study protocol was approved by the Committee on the  
120 Ethics of Animal Experiments of the INIA (Madrid, Spain; permit number CEEA  
121 2014/025).

122

123 **Experimental design**

124 *Comparison of the selection performed by different sperm preparation techniques in*  
125 *split semen samples using frozen-thawed and fresh human spermatozoa .*

126 In this experiment, we aimed to compare the selection performed by the current  
127 standard procedures for sperm selection, namely density gradient and swim-up, with the  
128 selection performed by rheotaxis using a proprietary designed microfluidic system. A  
129 control group of non-selected spermatozoa was also included, and sperm quality was  
130 assessed in terms of motility, morphology, and DNA fragmentation. Ten  
131 replicates/donors were assessed with frozen-thawed spermatozoa, and ten  
132 replicates/donors were assessed with fresh sperm cells. A replicate for frozen-thawed  
133 semen was a pool of 3 straws (1 from each of 3 ejaculates) from each donor while for  
134 fresh semen a replicate was 1 ejaculate per donor.

135 Next, to confirm the improvement in sperm morphology, we conducted a morphology  
136 evaluation at high magnification in frozen-thawed human sperm samples. For this,  
137 samples from three different ejaculates of each donor were thawed and pooled, the  
138 experiment was replicated 4 times with different donors, and at least 200 spermatozoa  
139 were assessed per sample. Additionally, to further characterise the selection performed  
140 by the above-mentioned sperm preparation methods, viability, membrane fluidity and  
141 acrosome integrity of frozen-thawed human spermatozoa were analysed by flow  
142 cytometry. This experiment had 12 replicates/donors and at least 10,000 events were  
143 analysed per sample.

144

145 *ICSI, in vitro culture and embryo transfers using a mouse model.*

146 After we demonstrated that human spermatozoa selected by rheotaxis displayed better  
147 motility, morphology and lower DNA fragmentation than spermatozoa selected using

148 current techniques, we used the mouse (*Mus musculus*) as a model to assess fertilization  
149 and embryo development rates after ICSI (Yanagimachi, 1998; Lyu *et al.*, 2010; Ma *et*  
150 *al.*, 2020).

151 We compared spermatozoa sorted using rheotaxis with the technique routinely used for  
152 the preparation of mouse sperm cells for ICSI, namely swim-up (n=10 males), and we  
153 completed ICSI of mouse oocytes (n=944 oocytes), *in vitro* culture and embryo  
154 transfers (n=25 over 10 days). The technician selecting spermatozoa for ICSI was  
155 blinded to the selection method.

156

### 157 **Semen samples**

158 Semen samples were donated by healthy donors after presenting for semen assessment  
159 at a fertility clinic. Samples were obtained by masturbation after 3–5 days of sexual  
160 abstinence and were processed and assessed in accordance with the WHO Guidelines  
161 (World Health Organization, 2010). Samples were allowed to liquefy at room  
162 temperature (RT; approximately 22 °C) for 30-60 min prior to processing. The transport  
163 to the laboratory was performed at RT and the same temperature was used to hold the  
164 samples while the sperm aliquots were distributed to the experimental groups. The  
165 inclusion criteria for semen samples were as follows: semen volume >1.5 mL, sperm  
166 concentration >15 x10<sup>6</sup> spermatozoa/mL, progressive motility >32% and normal forms  
167 >4%. Frozen human sperm samples were donated by Cryos International - Denmark  
168 ApS (Aarhus, Denmark). Briefly, following liquefaction of the semen samples obtained  
169 from selected healthy donors, one part of SpermCryo™ All-round (Gynotec, Malden,  
170 The Netherlands) was added to three parts of semen while gently swirling before  
171 leaving the sample for 10 min to equilibrate. The semen was transferred to CBS™ High  
172 Security straws (Cryo Bio Systems, L'Aigle, France), frozen in liquid nitrogen vapour

173 and stored at -196 °C. For each replicate one straw from each of three different  
174 ejaculates from the same donor were thawed (30°C for 30 s), pooled to avoid intra-  
175 individual differences and diluted 1:1 in sperm washing medium (SWM;  
176 PureSperm®Wash, Nidacon, Mölndal, Sweden). All experiments were completed  
177 blinded to the evaluator within 1 h after sperm collection/thawing.

178

## 179 **Sperm preparation techniques**

### 180 *Density gradient centrifugation*

181 A density gradient was prepared in a 15-mL conical tube by layering 2 mL of 40% (v/v)  
182 density gradient medium (PureSperm®40, Nidacon) over 2 mL of 80% (v/v) density  
183 gradient medium (PureSperm®80, Nidacon). An aliquot of 500 µL of semen was placed  
184 above the density gradient and centrifuged at 300g for 20 min. Following removal of the  
185 supernatant, the sperm pellet was resuspended in 5 mL SWM after which the pellet was  
186 disturbed by gentle pipetting and centrifuged at 500g for 10 min. Following  
187 centrifugation, the final pellet was resuspended in 500 µL SWM.

188

### 189 *Swim-up*

190 To select spermatozoa by the swim-up method, a semen aliquot of 500 µL was carefully  
191 pipetted under 1.5 mL SWM in a sterile 15 mL conical tube. The falcon tube was  
192 inclined at an angle of 45° to increase the surface area of the semen-culture medium  
193 interface and was incubated for 1 h at 37 °C in a water bath. Afterwards, the tube was  
194 returned to the upright position, and the uppermost 1 mL of medium was collected,  
195 transferred to a new tube and centrifuged at 500g for 10 min. Finally, the supernatant  
196 was discarded, and the sperm pellet was resuspended in 500 µL SWM.

197



198 ***Microfluidic chip***

199 A disposable device with a microfluidic channel was manufactured by CNC machining  
200 from polymethyl methacrylate (PMMA). The microfluidic channel measured 300  $\mu\text{m}$   
201 wide, 100  $\mu\text{m}$  deep and 10 mm in length (Fig. 1). It was connected to a syringe pump  
202 (Standard Infuse/Withdraw PHD ULTRA™ Syringe Pump, Harvard Apparatus,  
203 Holliston, USA) by silicone tubing and a connector (Male Mini Luer fluid connector,  
204 Microfluidic ChipShop, Jena, Germany). The microfluidic channel was primed with  
205 SWM to remove air bubbles, following this, the flow velocity was stabilised at 30  $\mu\text{m}/\text{s}$ .  
206 A 20  $\mu\text{L}$  sperm sample was loaded into the starting inlet of the microfluidic channel  
207 allowing spermatozoa to orient against the oncoming flow and swim against it (positive  
208 rheotaxis) for 30 min. Sperm progression was assessed under 200X magnification on an  
209 inverted microscope (CK40; Olympus, Center Valley, USA). At the end of this period,  
210 spermatozoa that reached the collection wells (20  $\mu\text{L}$  per well) were collected and  
211 submitted to further analysis. For a more comprehensive understanding of the  
212 microfluidic device see Videos 1-5.

213

214 **Motility evaluation**

215 As part of the quality control, initial sperm motility was assessed within 30 min after  
216 liquefaction of the sample or thawing and pooling the straws. It was also evaluated after  
217 each sperm preparation technique. To this end, a volume of 10  $\mu\text{L}$  of semen was  
218 delivered onto a clean glass slide and covered with a 22 mm  $\times$  22 mm coverslip. The  
219 procedure was performed at 37°C with a heated microscope stage using a phase-contrast  
220 microscope (BX60; Olympus) equipped with an eyepiece reticle with grid at 200X  
221 magnification. Motility was assessed as follows; (i) progressive motility (PR):  
222 spermatozoa moving actively, either linearly or in a large circle, regardless of speed, (ii)

223 non-progressive motility (NP): all other patterns of motility with an absence of  
224 progression, and (iii) immotility (IM): no movement. At least 200 spermatozoa were  
225 scored per replicate for the percentage of different motile categories.

226

### 227 **Morphology evaluation**

228 To determine sperm morphology, a 10  $\mu$ L aliquot of the sperm preparation was smeared  
229 onto a clean slide, allowed to dry in air and stained using the Diff-Quik kit (RAL  
230 Diagnostics, Martillac, France). The slide was examined immediately after drying, with  
231 brightfield optics at 1000X magnification using oil immersion. A normal/abnormal  
232 classification, along with a detailed recording of the location of sperm abnormalities,  
233 was performed following the criteria proposed in the 5<sup>th</sup> edition of the WHO guidelines  
234 (World Health Organization, 2010). The following categories of defects were noted; (i)  
235 head defects, (ii) neck and midpiece defects, (iii) principal piece defects, and (iv) excess  
236 residual cytoplasm. A minimum of 200 spermatozoa were evaluated in each replicate.

237

### 238 **Morphology evaluation at high magnification**

239 Spermatozoa (frozen-thawed only) were visualised using a 60X objective on a  
240 Nomarski differential interference contrast (DIC) inverted microscope (Nikon Eclipse  
241 Ti, Nikon Instruments Europe BV, Amsterdam, Netherlands) equipped with a specific  
242 package for intracytoplasmic morphologically selected sperm injection (IMSI; RI IMSI,  
243 Research Instruments Ltd, Cornwall, UK) and further magnified using RI Viewer  
244 software up to 6000X. Spermatozoa were graded and classified into four groups  
245 according to the presence or size of vacuoles following the criteria described by  
246 Vanderzwalmen *et al.*, (2008): (i) Grade I, absence of vacuoles; (ii) Grade II, maximum  
247 of two small vacuoles; (iii) Grade III, more than two small vacuoles or at least one large

248 vacuole; and (iv) Grade IV, large vacuoles in conjunction with abnormal head shapes or  
249 other abnormalities.

250

#### 251 **DNA fragmentation assay**

252 Sperm DNA integrity was evaluated by the acridine orange (AO) test as described by  
253 Ajina et al., (2017). To avoid rapidly fading fluorescence, all the slides were observed  
254 within 5 min under a fluorescence microscope (BX60; Olympus) at 1000X  
255 magnification, with excitation at 450-490 nm. Spermatozoa with normal (double-  
256 stranded) DNA showed green fluorescence, and those with denatured or single-stranded  
257 DNA were red, orange, or yellow. The DFI (Jiang *et al.*, 2011) was used to represent the  
258 ratio of spermatozoa with red, orange, or yellow fluorescence relative to all the  
259 spermatozoa analysed per sample. At least 200 spermatozoa were assessed for each  
260 replicate.

261

#### 262 **Flow cytometry**

263 The aim of the flow cytometry analysis was to detect viability, membrane fluidity and  
264 acrosome integrity in spermatozoa (frozen-thawed only) selected by the different sperm  
265 preparation techniques. In all samples, the sperm concentration was set at  $1 \times 10^6$   
266 spermatozoa per mL and sperm suspension was incubated with a three stain  
267 combination of fluorochromes Yo-Pro1 (15nM, ThermoFisher Scientific, Waltham,  
268 USA), Merocyanine M540 (2.6  $\mu$ M, Sigma-Aldrich) and Lectin PNA from *Arachis*  
269 *hypogaea* conjugated with Alexa Fluor™ 647 (2.5  $\mu$ g/mL, ThermoFisher Scientific) for  
270 15 min at 37°C. Subsequently, samples were subjected to analysis by CytoFlex flow  
271 cytometry (Beckman Coulter Inc., Brea, USA) equipped with violet (405 nm), blue (488  
272 nm) and red (635 nm) lasers. Sperm population was discriminated from debris with the

273 forward scatter (FSC) and side scatter (SSC) signals. Yo-Pro1 and M540 were excited  
274 with the 488nm laser, while PNA-A647 was excited with the 635nm laser and emission  
275 was detected by the 525/40BP, 585/42BP and 690/50BP filters, respectively. The  
276 analysis of the flow cytometry data was carried out using CytExpert, version 2.3.0.84  
277 (Beckman Coulter Inc.). All variables were assessed using logarithmic amplification,  
278 10,000 gated events were collected for each sample and flow cytometry data are  
279 expressed as percentage from the total analysed population.

280

### 281 **Animals, Gamete Collection, and Sperm Freezing**

282 Both male and female mice were fed ad libitum with a standard diet and maintained in a  
283 temperature-and light-controlled room (23 °C, 14L:10D). When required, animals were  
284 euthanised by cervical dislocation.

285

286 Spermatozoa were collected from the caudal epididymis of 3-month-old B6D2 males  
287 (F1 hybrid of C57BL/6J females and DBA/2J males) and suspended in a non-  
288 capacitating modified human tubal fluid medium (ncHTF)(Pérez-Cerezales *et al.*, 2018).  
289 The pH of the ncHTF medium was adjusted to 7.4 and spermatozoa were incubated for  
290 1 h at 37 °C without CO<sub>2</sub> to allow motile spermatozoa to swim to the surface of the  
291 droplet. Following sperm collection and transfer to a sterile Eppendorf tube, the sample  
292 was either subjected to sperm selection using the microfluidic channel described earlier  
293 (rheotaxis) or not (swim-up). Once selected, sperm samples were frozen by immersion  
294 in liquid nitrogen (Lacham-Kaplan *et al.*, 2003) and stored for periods ranging from 1  
295 day to 4 weeks at -80 °C. Frozen-thawed spermatozoa were mixed with 40-50 µL of a  
296 10% polyvinyl-pyrrolidone (PVP-360) in M2 medium before being placed in the culture  
297 dish for microinjection.

298

299 *Mouse oocyte collection.* Metaphase II oocytes were collected from the oviducts of 6- to  
300 8-wk-old B6D2 female mice superovulated with 7.5 IU of eCG, and with an equivalent  
301 dose of hCG 48 h later, as described by Fernández-González et al., (2008).

302

### 303 **Intracytoplasmic sperm injection in mice**

304 ICSI with frozen-thawed mouse spermatozoa was performed in M2 medium at RT, as  
305 previously described (Moreira *et al.*, 2007). Individual sperm heads decapitated by the  
306 snap-freezing procedure were injected into oocytes. Oocytes were injected in groups of  
307 10 per treatment with spermatozoa from one male.

308

### 309 **In vitro embryo culture**

310 After 15 min of recovery at 37 °C in M2 medium, surviving oocytes were returned to  
311 mineral oil-covered KSOM and cultured in groups of 20-40 embryos in 25 µl drops at  
312 37 °C in a 5% CO<sub>2</sub> atmosphere. Fertilization was evaluated as the percentage of  
313 embryos reaching the 2-cell stage (Cleavage rate) after 24 h in culture.

314

### 315 **Embryo transfer**

316 Embryo transfer was performed as described previously (Fernández-Gonzalez *et al.*,  
317 2008). Briefly, recipient pseudopregnant females (CD1 females mated with  
318 vasectomized males) 0.5 days post coitum were anaesthetised with inhaled isoflurane and  
319 2-cell embryos were transferred into the oviducts. Each female received 10-12 embryos  
320 from both treatments into either the left or right oviducts. On day 15 days after ICSI,  
321 surrogate females were euthanised and the number of foetuses and reabsorptions were  
322 scored as described by Perez-Cerezales et al, (2018). Subsequently, the percentage of

323 transferred embryos implanted (Implantation rate) and the percentage of implanted  
324 embryos developed until the foetus stage (Foetus development rate) were calculated.

325

### 326 **Statistical analysis**

327 Data were analysed using Statistical Package for the Social Sciences (SPSS) (version  
328 25, IBM, Chicago, USA). Data were first examined for normality of distribution using  
329 the Shapiro-Wilk test and later for homogeneity of variance using Levene's test.  
330 Unpaired t-tests for independent samples were performed for simple two-group  
331 comparisons. For group-wise comparisons a univariate analysis of variance (ANOVA)  
332 was used. Post hoc tests were conducted using the Bonferroni test. Results were  
333 reported as the mean  $\pm$  standard error of the mean (s.e.m).  $P < 0.05$  was considered  
334 statistically significant.

335

## 336 **RESULTS**

### 337 **Comparison of the selection performed by different sperm preparation techniques 338 in split semen samples using frozen-thawed and fresh human spermatozoa.**

339 Firstly, the motility of the samples was assessed, and total motility (TM, %) was  
340 calculated as follows:  $TM = PR + NP$ . Spermatozoa selected by rheotaxis had higher TM  
341 than the other selection techniques studied, both with frozen and fresh samples ( $P <$   
342  $0.001$ ; Fig. 2A, Fig. 2B, respectively). The swim-up selection also increased TM when  
343 compared to density gradient and control groups, irrespective of whether they were  
344 frozen-thawed or fresh ( $P < 0.001$ ). However, surprisingly, no significant improvement  
345 in TM was achieved through the density gradient in both frozen-thawed and fresh  
346 spermatozoa.

347

348 Subsequently, we analysed the levels of DNA fragmentation of the sperm samples and  
349 calculated the DFI. In frozen-thawed samples (Fig. 2C), the level of DNA fragmentation  
350 of the initial samples ( $18.0 \pm 4.9$ ) was only reduced by rheotaxis selection ( $13.2 \pm 4.6$   
351 lower;  $P < 0.05$ ). This trend was also evident with fresh samples (Fig. 2D) where the  
352 initial DFI of the samples ( $10.3 \pm 2.3$ ) was reduced by rheotaxis selection ( $8.6 \pm 1.4$   
353 lower;  $P < 0.05$ ), but also through the selection achieved with the swim-up ( $6.9 \pm 1.2$   
354 lower;  $P < 0.05$ ).

355

356 Samples were also stained to assess sperm morphology. In frozen-thawed samples (Fig.  
357 2E), we found that selection by rheotaxis improved the percentage of spermatozoa with  
358 normal morphology (NM;  $40.5 \pm 5.8$  higher;  $P < 0.001$ ), while no improvement was  
359 achieved by density gradient or swim-up selection. In addition, when sperm  
360 morphology of fresh samples was assessed after performing the selection procedures  
361 (Fig. 2F), selection by rheotaxis not only increased NM from the starting population  
362 ( $49.2 \pm 2.9$  higher;  $P < 0.001$ ), but also yielded a superior NM than density gradient and  
363 swim-up ( $41.5 \pm 3.8$  and  $39.2 \pm 3.6$  higher, respectively;  $P < 0.05$ ).

364

365 The type of sperm morphological abnormalities was also characterised (Table 1). In  
366 frozen-thawed and fresh samples, rheotaxis selected spermatozoa had fewer head  
367 abnormalities, in comparison to control, density gradient and swim-up ( $P < 0.05$ ). A  
368 similar trend was observed in midpiece defects, but no further reduction was obtained  
369 when comparing gradient vs. rheotaxis in frozen-thawed samples. None of the selection  
370 techniques affected abnormalities relating to the principal piece and excess residual  
371 cytoplasm in frozen-thawed samples. However, in fresh samples, sperm rheotaxis and  
372 swim-up selection reduced the presence of abnormalities in the principal piece ( $P <$

373 0.001), while the presence of excess residual cytoplasm decreased with the three  
374 selection techniques studied ( $P < 0.001$ ).

375

376 When sperm morphology was evaluated at high magnification, spermatozoa were  
377 graded into four groups according to the presence or size of the vacuoles, however, as  
378 Grade I and Grade II (absence of vacuoles and maximum of two small vacuoles,  
379 respectively) are deemed acceptable for ICSI, in Fig. 3 we present the percentage of  
380 Grade I + Grade II together. Sperm selection by rheotaxis increased the percentage of  
381 Grade I+II spermatozoa in comparison to the starting unselected sperm population,  
382 density gradient and swim-up ( $P < 0.001$ ).

383

384 When sperm subjected to flow cytometry were classified based on the fluorescence of  
385 Yo-Pro-1, the percentage of viable spermatozoa after density gradient centrifugation  
386 was similar to the neat sample. However, spermatozoa processed either by swim-up or  
387 rheotaxis had increased sperm viability ( $19.5 \pm 3.5$  and  $35.5 \pm 4.2$  % higher,  
388 respectively), with the latter having the highest increase (Fig. 4A;  $P < 0.01$ ). The  
389 population of sperm selected by rheotaxis had similar acrosome integrity to the other  
390 treatments ( $P > 0.05$ ) (Fig. 4B). Rheotactically selected sperm exhibited a similar  
391 membrane fluidity profile to swim-up selected sperm, but was lower than that of the  
392 neat sample as well as density gradient selected sperm (Fig. 4C;  $P < 0.001$ ).

393

#### 394 **ICSI, in vitro culture and embryo transfer in a mouse model.**

395 Using a mouse model, we have demonstrated that when mouse spermatozoa were  
396 selected using rheotaxis or swim-up, there was a significant increase in fertilization  
397 rates following ICSI, evaluated as the percentage of embryos reaching the 2-cell stage



398 ( $P < 0.01$ ; Fig. 5A). The resultant embryos were then transferred to recipient females  
399 and those fertilized using rheotactically selected spermatozoa had a 12% higher  
400 implantation rate ( $P < 0.001$ ; Fig. 5B) and a 20% higher foetal development rate ( $P <$   
401  $0.05$ ; Fig. 5C).

402

## 403 **DISCUSSION**

404 Using both fresh and frozen-thawed spermatozoa, we have applied a novel simple  
405 method which can provide the embryologist with a population of sperm cells with  
406 superior DNA integrity as well as improved morphology and motility than the currently  
407 used methods of density gradient and swim-up. When mouse spermatozoa were selected  
408 using rheotaxis, it yielded higher fertilisation and implantation rates than when  
409 spermatozoa were selected using swim-up, and the offspring had normal embryonic  
410 development. Critically this biomimicry process does not involve centrifugation of  
411 spermatozoa or the use of exogenous binding substances.

412

413 Since the successful application of ICSI in 1992 to treat male factor infertility (Palermo  
414 *et al.*, 1992), there has been a lack of an efficient physiological method for selecting the  
415 most suitable spermatozoon to be injected into a mature oocyte. The predominance of  
416 ICSI over IVF (De Geyter *et al.*, 2020), is increasing the need to replace the traditional  
417 and rudimentary sperm preparation techniques (density gradient and swim-up).  
418 Mimicking the journey spermatozoa would undergo on their way to the fallopian tubes  
419 *in vivo* and based on rheotaxis, a natural functional test of swimming against a flow, we  
420 have developed a technology to help the embryologists to select the best sperm cells for  
421 ICSI.

422

423 Similar to Yamanaka *et al.*, (2016), the percentage of motile spermatozoa in samples  
424 processed by density gradient in this study was similar to that in the original semen but  
425 increased with swim-up. Moreover, our device increased the total motility of the  
426 sample, both with frozen and fresh semen compared to the other selection techniques  
427 studied. A similar improvement was achieved by other authors who compared  
428 microfluidic sperm sorters with the sperm preparation procedure of density gradient  
429 centrifugation combined with swim-up; 100 versus 91% progressive motility,  
430 respectively, in Quinn *et al.*, (2018), or 95.4 versus 60.3% total motility, respectively, in  
431 Shirota *et al.*, (2016).

432

433 Our rheotactically driven selection not only has increased the percentage of selected  
434 spermatozoa with normal morphology, both in fresh and frozen-thawed samples, but  
435 also, yielded a higher percentage of normal morphology than density gradient and  
436 swim-up (3 and 2 to 3-fold, respectively). We have also shown that rheotaxis selected  
437 spermatozoa had fewer head abnormalities, in comparison to control, density gradient  
438 and swim-up. Moreover, when sperm morphology was evaluated at high magnification,  
439 sperm selection by rheotaxis increased the percentage of spermatozoa with normal head  
440 morphology and no or small vacuoles (Grades I-II) in comparison to the starting  
441 unselected sperm population, density gradient and swim-up. The selection of  
442 spermatozoa for ICSI with normal head morphology and size at high magnification has  
443 been reported to be associated with improved fertilization (Cassuto *et al.*, 2009),  
444 blastocyst development (Vanderzwalmen *et al.*, 2008), implantation and pregnancy rates  
445 (Hazout *et al.*, 2006), as well as lower miscarriage rates (Antinori *et al.*, 2008).

446

447 Nowadays, all the techniques to evaluate sperm DNA integrity render the sperm cells  
448 non-usable for human application. In cases where high levels of DNA fragmentation are  
449 diagnosed, the chance of spontaneous conception declines at sperm DFI values above  
450 20% and approaches zero for values over 30-40% (Cissen *et al.*, 2016). Our device  
451 selected a sperm population with decreased levels of DNA fragmentation for both fresh  
452 and frozen samples, as assessed by DFI. This is in agreement with other authors that  
453 have reported less DNA fragmentation in spermatozoa sorted using microfluidic devices  
454 (Kishi *et al.*, 2015; Shirota *et al.*, 2016). Shirota *et al.*, (2016) reported a significantly  
455 lower sperm DFI with a microfluidic chip compared with a centrifugation plus swim-up  
456 procedure (0.8 vs 10.1%, respectively). Regarding the traditional sperm preparation  
457 techniques, we found that only the swim-up method could reduce DFI, at least with  
458 fresh sperm samples. A similar reduction was recently reported by Oguz *et al.*, (2018)  
459 who showed that swim-up but not density gradient method yielded a significant  
460 reduction in the DFI compared to basal rates, in semen samples of both unexplained and  
461 mild male factor subgroups. These results partially agree with other authors who  
462 reported DFI was reduced with density gradient, but unsurprisingly swim-up alone or  
463 density gradient followed by swim-up yielded greater reductions in DFI (Volpes *et al.*,  
464 2016; Yamanaka *et al.*, 2016).

465

466 Unfortunately, the literature regarding a deep sperm characterisation after different  
467 sperm preparation techniques in human species is scarce and it is infrequent to have  
468 other parameters analysed apart from motility, morphology and DNA fragmentation. In  
469 this regard, we report here that, among the sperm selection techniques, rheotaxis  
470 selected a population of spermatozoa with the highest viability, being even higher than  
471 the improvement shown by the swim-up technique and which had been previously

472 reported (Force *et al.*, 2001; Ricci *et al.*, 2009; Highland *et al.*, 2016). Moreover, when  
473 sperm plasma membrane fluidity was analysed to detect early signals of sperm  
474 capacitation (reviewed by Leahy and Gadella, 2015), we report the same degree of  
475 membrane fluidity for the traditional sperm preparation techniques and the neat sample,  
476 but not for rheotaxis, which showed a slightly higher percentage of spermatozoa with  
477 low membrane fluidity. The results of the current study are in line with previous reports  
478 in which under non capacitating conditions, similar to ours, there was no increase in  
479 membrane fluidity between the neat sample and the sperm population selected by  
480 density gradient centrifugation (Buffone *et al.*, 2009) or swim up (Force *et al.*, 2001).  
481 Zhang *et al.*, (2016) reported that there is no active signal transduction during human  
482 sperm rheotaxis, as it is a passive process, resulting from hydrodynamic interactions  
483 between the sperm flagellum and the surrounding fluid flow, where without extra  
484 energy consumption, sperm can reserve energy for executing later important events  
485 prior to fertilization.

486

487 Using mouse oocytes, we demonstrated that when mouse spermatozoa were selected for  
488 ICSI using rheotaxis compared to the swim-up method, there was a significant increase  
489 in fertilization rate. This improvement was also reflected by increased implantation and  
490 development until the foetal stage after transferring the embryos to recipient females.  
491 This may be due to spermatozoa with lower levels of DNA fragmentation being used in  
492 the rheotaxis treatment. A similar experimental approach was recently used to  
493 demonstrate an improved ICSI efficiency and a rise in the embryo quality with mouse  
494 spermatozoa selected by thermotaxis (Pérez-Cerezales *et al.*, 2018), which lead us to  
495 validate not only the use of the mouse model for obtaining data on fertilization,

496 implantation and foetal development, but also the safety of this method of sperm  
497 selection.

498

#### 499 **Conclusion**

500 Here we report a single-use novel microfluidic device that stimulates spermatozoa to  
501 swim against a flow of media driven by an electronic syringe pump. Over a 30 min  
502 period spermatozoa swim into a collection well from where a highly selected sperm  
503 fraction with low DFI can be removed and used for ICSI. This method selects  
504 spermatozoa not only with lower DNA fragmentation but also with higher motility,  
505 morphology and viability than currently used sperm selection methods in clinical  
506 practice. In addition, it has the potential to significantly reduce the time embryologists  
507 spend preparing the sample and selecting sperm for treatment. Using a mouse ICSI  
508 model, we have reported significantly improved fertilization and embryo development  
509 rates. Further studies should be performed in fertility clinics to provide clinical data on  
510 the benefit of this sperm preparation method.

511

#### 512 **DECLARATION OF INTEREST**

513 The authors declare that there is no conflict of interest that could be perceived as  
514 prejudicing the impartiality of the research reported.

515

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518

#### 519 **AUTHOR CONTRIBUTION STATEMENT**

520 JR contributed to the design of the study, performed the experiments, analysed the data,  
521 and drafted the manuscript. RL and RF carried out the ICSI and the embryo transfers in  
522 mice. MS performed and analysed the flow cytometry experiments. FW contributed to  
523 the design of the experiments with human sperm samples and conducted the  
524 morphology evaluation at high magnification. JC, DM and PBL provided human semen  
525 samples and contributed to the design of the experiments with the human sperm  
526 samples. AGA designed and analysed the mouse ICSI and embryo transfer experiments  
527 while AMG contributed to the interpretation of the data. DN secured funding for the  
528 work, contributed to the design of the microfluidics system and the experiments. SF  
529 secured funding for the work, conceived and designed the study, analysed the data, and  
530 edited the manuscript. All authors read and revised the article and approved the final  
531 manuscript.

532

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537

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701  
702

703 **FIGURE LEGENDS**

704

705 **Figure 1. Microfluidic chip.**

706 A disposable chip with a microfluidic channel was manufactured from polymethyl  
707 methacrylate (PMMA). (a) The microfluidic channel measured 300  $\mu\text{m}$  wide, 100  $\mu\text{m}$   
708 deep and 10 mm in length. (b) It was connected to a syringe pump (Standard  
709 Infuse/Withdraw PHD ULTRA™ Syringe Pump, Harvard Apparatus, Holliston, USA)  
710 by silicone tubing and a connector (Male Mini Luer fluid connector, Microfluidic  
711 ChipShop, Jena, Germany). The microfluidic channel was primed with sperm washing  
712 medium (PureSperm®Wash, Nidacon, Mölndal, Sweden) to remove air bubbles,  
713 following this, the flow velocity was stabilised at 30  $\mu\text{m}/\text{s}$ . (c) A 20  $\mu\text{L}$  sperm sample  
714 was loaded into the starting inlet of the microfluidic channel allowing spermatozoa to  
715 orient against the oncoming flow and swim against it (positive rheotaxis) for 30 min.  
716 Sperm progression was assessed under 200X magnification on an inverted microscope  
717 (CK40; Olympus, Center Valley, USA). (d) At the end of this period, spermatozoa that  
718 reached the collection wells were collected and submitted to further analysis. (e) Waste  
719 well.

720

721 **Figure 2. Motility, DNA fragmentation and morphology of frozen-thawed and**  
722 **fresh human spermatozoa by the method of processing.**

723 Total motility (a and b), DNA fragmentation index (DFI; c and d) and normal  
724 morphology (e and f) of frozen-thawed (a, c and e) and fresh (b, d and f) human  
725 spermatozoa selected by density gradient (gradient), swim-up or rheotaxis. Non selected  
726 (control) treatment is also represented. Each bar is a mean  $\pm$  s.e.m of the 10  
727 replicates/donors. <sup>abc</sup>Differing superscripts differ significantly.

728

729 **Figure 3. Frozen-thawed human sperm morphology evaluated at high**  
730 **magnification (6000X).**

731 Spermatozoa selected by density gradient (gradient), swim-up, rheotaxis, or non-  
732 selected (control) spermatozoa were graded and classified into four groups according to  
733 the presence or size of vacuoles following the criteria described by Vanderzwalmen *et*  
734 *al.*, (2008). As only grade I and II are suitable for use in ICSI, the percentage of Grade I  
735 + Grade II are shown together. Samples from three different ejaculates of each donor  
736 were thawed and pooled, the experiment was replicated 4 times with different donors,  
737 and at least 200 spermatozoa were assessed per donor/sample. Each bar is a mean  $\pm$   
738 s.e.m of the 4 replicates. <sup>abc</sup>Differing superscripts differ significantly ( $P < 0.001$ ).

739

740 **Figure 4. Viability, acrosome integrity and membrane fluidity of frozen-thawed**  
741 **human spermatozoa evaluated by flow cytometry.**

742 Viability (denoted a), acrosome integrity (denoted b) and membrane fluidity (denoted c)  
743 of frozen-thawed human spermatozoa selected by density gradient (gradient), swim-up  
744 or rheotaxis. Non selected (control) treatment is also represented. Data are expressed as  
745 percentage from the total analysed population. Each bar is a mean  $\pm$  s.e.m of the 12  
746 replicates/donors. <sup>abc</sup>Differing superscripts differ significantly ( $P < 0.05$ ).

747

748

749 **Figure 5. Cleavage, implantation, and foetal development rates following**  
750 **intracytoplasmic sperm injection of mouse spermatozoa preselected by swim-up or**  
751 **rheotaxis.**

752 Fertilization was evaluated as the percentage of embryos reaching the 2-cell stage  
753 (Cleavage rate; denoted a). Subsequently, after transferring the embryos to recipient  
754 females, the percentage of embryos implanted (Implantation rate; denoted b) and the  
755 percentage of embryos developed until the foetus stage (Foetus development rate;  
756 denoted c) were calculated. Twenty replicates were completed using a total of 944  
757 oocytes and spermatozoa from 10 males. Embryos reaching the 2-cell stage were  
758 transferred to 25 females. Each female received 10-12 embryos from both treatments  
759 into either the left or right oviducts. Females were sacrificed at D14 of gestation.  
760 Vertical bars represent mean  $\pm$  s.e.m. \*\*Differing superscripts differ significantly.

761



762 **VIDEO LEGENDS**

763

764 **Video 1. Start of the microfluidic channel demonstrating how human spermatozoa**  
765 **gain entry into the channel.** Arrow indicates the direction of the flow. An asterisk  
766 indicates the starting well. Sperm progression was recorded under 100X magnification  
767 on an inverted microscope (CK40; Olympus, Center Valley, USA).

768

769 **Video 2. Middle of the microfluidic channel showing how human spermatozoa**  
770 **progress upstream.** Arrow indicates the direction of the flow. Sperm progression was  
771 recorded under 200X magnification on an inverted microscope (CK40; Olympus,  
772 Center Valley, USA).

773

774 **Video 3. The lateral channel of the microfluidic device showing how human**  
775 **spermatozoa progress through it.** Sperm progression was recorded under 200X  
776 magnification on an inverted microscope (CK40; Olympus, Center Valley, USA).

777

778 **Video 4. End of the lateral channel of the microfluidic device showing how human**  
779 **spermatozoa advance into the collection zone/well.** An asterisk indicates the  
780 collection well. Sperm progression was recorded under 200X magnification on an  
781 inverted microscope (CK40; Olympus, Center Valley, USA).

782

783 **Video 5. Selected human sperm population at the collection well of the microfluidic**  
784 **device.** Sperm progression was recorded under 100X magnification on an inverted  
785 microscope (CK40; Olympus, Center Valley, USA).